Fractional laser treatment for medical skin diseases

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Not just for aesthetic procedures, fractional photothermolysis can be used for a range of medical skin conditions. Dieter Manstein, Daniel Karasik and Neera Nathan from Harvard Medical School explain the treatment and its role in medical dermatology.

In 2004, the concept of fractional photothermolysis (FP) was introduced and revolutionised the field of laser dermatology [1]. By creating a pattern of microscopic thermal wounds, this laser technology largely replaced fully ablative lasers for the treatment of photoaged skin due to a milder side-effect profile and faster recovery period. While FP was initially purposed for aesthetics, there has been mounting clinical and histopathological evidence that it may be used as a monotherapy or as an adjuvant therapy to treat a wide variety of medical skin conditions. Herein, we describe the concept of FP and report notable uses in medical dermatology.

Fractional photothermolysis
FP refers to the application of small-diameter laser exposures to the skin in order to create an array of microscopic treatment zones (MTZ) of thermal injury between healthy and intact skin [1]. A critical difference between FP and conventional ablative and non-ablative lasers is that whereas conventional lasers treat large, uninterrupted areas of the skin, FP creates a discrete pattern of defined coagulated tissue surrounded by healthy tissue, which may serve as a reservoir to promote wound healing and tissue repair (Figure 1).

These patterns of MTZs exhibit at least 200 to 300μm between each MTZ, and the diameter of each MTZ is usually less than approximately 400μm [2] with a lesion depth that can extend to the reticular dermis. MTZ diameter and depth is controlled by adjusting the laser energy settings while the wavelength and optical configuration is typically fixed and predetermined for each FP device. Density of treatment, defined as number of MTZs per cm², is generally referred to as the percentage-of-coverage, or the percent of damaged dermis within a defined treatment area [2]. The MTZ density of treatment per single pass varies according to either adjustment of the placement mechanism within the handpiece, or for some devices, by selecting between different handpieces with a specific preset MTZ density. A single pass generally has a density of as low as 1% to 30%, and increasing the number of passes, and occasionally, the energy level, can increase the density of the skin treated. As such, energy settings per pulse and density are the primary input parameters for FP treatment [2]. The histological damage profile is also affected by the device-specific optics and temporal pulse profile (mainly the pulse duration). The laser user should be aware that the treatment densities are not necessarily consistent across manufacturers. As the methods to determine the treatment density differ (e.g. histological assessment, burn paper coverage test, tongue depressor test, etc.), the treatment outcome between devices from different manufacturers also likely differ, even if the same wavelength, energy and treatment density are applied.

FP can be characterised into ablative (aFP) [3] and non-ablative FP (nFP). Ablative FP is characterised by actual tissue removal within the MTZ by focused laser radiation, resulting in a small diameter hole of varying, energy-determined depth. This hole is surrounded by a small cuff of thermally coagulated tissue. Typically, far infrared lasers, like carbon dioxide (CO2) or erbium-doped yttrium aluminium garnet (Er:YAG) lasers with strong absorption in tissue, are used to create ablative MTZs. Non-ablative FP is characterised by the application of 1440-1550-nm infrared lasers, and 1927-nm Thulium lasers [4], which are more moderately absorbed and therefore do not result in actual laser drills, but rather columns of tissue coagulation with varying, energy-dependent depths.

The MTZs created by the aFP treatment compromise the dermal-epidermal junction (DEJ) (Figure 2), thereby allowing for dermal debris to be removed through it [5]. With nFP treatment, microscopic epidermal necrotic debris (MENDs) can be seen. MENDs contain melanin pigment, and may act as a melanin shuttle as soon as one day post-treatment [6], a mechanism that aids in the ability of nFP to treat photoaged or hyperpigmented skin. Additionally, nFP treatment results in a wound healing response in the dermis. This is evident through expression of heat shock protein.
complications associated with FP is lower: a 2010 review noted that although overall rate of adverse events have been reported. Avram et al. (2009) reported hypertrophic scarring due to aFP treatment for photoaged skin on the neck of five patients, though early diagnosis and proper treatment successfully reversed the damage in this case [11]. A 2010 review noted that although overall rate of complications associated with FP is lower than traditional ablative laser treatments, serious complications may still occur, including prolonged (>4 days) erythema, herpes simplex virus (HSV) infection (in 0.3% to 2% of cases), post-inflammatory hyperpigmentation (PIH), and scarring, among other complications [12]. Special attention to sensitive sites, and by pairing high energy settings with low treatment density, and vice versa, may help limit some of these complications.

### Laser-assisted drug delivery

An important application of aFP treatment for conditions in medical dermatology is laser-assisted drug delivery (LADD). Whereas cutaneous bioavailability of topical drugs is relatively low, as only around 1-5% of a drug is naturally absorbed through the skin, ablative fractional lasers may help to increase overall topical drug absorption to intended targets in the dermis [13]. By breaking down portions of the stratum corneum, the premier barrier of the skin, the delivery of even large molecules and particles into the skin is possible. Laser settings and parameters can be modified for more or less ablation commensurate to desired quantity of drug delivery [13]. Perhaps the most widely used application of LADD is the use of triamcinolone solution following ablative fractional laser treatment for even improvement of scars [14,15]. Further, LADD has been shown to be an effective way to increase the penetration of topical 5-fluorouracil for the treatment of non-melanoma skin cancer [16], among other indications where increasing drug bioavailability may be synergistic with the tissue effects of the laser, including verruca vulgaris [17], macular amyloidosis [18], onychomycosis [19], facial papules [20] and psoriasis [21,22].

### Uses in medical dermatology

#### Disorders of connective tissue

There is accumulating evidence that fractional lasers may improve the clinical and histologic appearance of scars, including hypertrophic scars and keloids [23,24]. FP is an effective treatment for traumatic scars, including as a single modality treatment, to enhance delivery of topical or injectable agents, and as an adjunctive therapy to surgery [14]. In addition to scar appearance, FP has been shown to improve scar texture, pain and itch, notably in burn scars, despite heterogeneous quality [25,26]. A very recent consensus statement reported that ablative fractional lasers are the overall preferred single modality treatment for traumatic scars [14].

FP has also been shown to improve sclerotic conditions, including scleroderma and chronic-graft-versus-host disease, which are characterised by thick, homogenised collagen. This includes improvement of contractures and range of motion when performed over focal areas in several case reports and case series [27-29].

Further, fractional ablative CO2 laser treatment significantly thinned collagen on histopathological examination and increased patient satisfaction compared to low dose UVA-1 therapy in localised scleroderma patients [30].

In addition to the conditions listed above, which are characterised by an excess of collagen, FP has been shown in various clinical studies to also treat conditions with an abnormal loss of collagen, including depressed acne scars [31-34] and other atrophic scars [35, 36]. Additionally, FP appears to improve disorders of elastic tissue quantity and / or quantity, including striae distensae, and in particular, stria alba [37,38]. Other elastic fibre disorders that were treated successfully with FP treatment include elastosis perforans serpiginosa treated with a fractional ablative CO2 laser [39], and pseudoxanthoma elasticum-like papillary dermal elastolysis and cutis laxa using non-ablative fractional lasers [40].

Depositional disorders that affect the connective tissue, including primary cutaneous amyloidosis, have also been shown improvement with fractional photothermolysis. This includes both clinical improvement and histologic reduction of amyloid deposits after treatment with fractional ablative CO2 laser with and without LADD of vitamin C and topical
steroids [18] in addition to treatment with a fractional non-ablative 1550-nm laser [41].

**Benign facial neoplasms**

FP has proven to be a useful tool in treating various benign facial neoplasms. For instance, FP treatment has been shown in several studies to help flatten facial angiofibromas in people with tuberous sclerosis complex as an adjunct therapy to other lasers, or to topical treatments such as sirolimus [20,42]. Additionally, treatment with an ablative fractional CO2 laser combined with a fully ablative CO2 laser was shown to successfully reduce trichodiscomas associated with Birt-Hogg-Dubé syndrome in one patient [43]. Ablative fractional CO2 lasers have also been shown to improve syringomas in 15/35 patients in one prospective cohort study [44].

**Pigmentary disorders**

FP appears to be a promising treatment for a broad range of pigmentary disorders, including those characterised by depigmentation, hypopigmentation and hyperpigmentation [45-50]. This includes vitiligo [45-47], idiopathic guttate hypomelanosis [49, 51], hypopigmented scars [50] and post-inflammatory hyperpigmentation [48]. FP treatment of melasma has yielded mixed results—some reports show that FP is an effective treatment modality, with and without the use of additional topical agents, [52-57] whereas one study does not recommend FP treatment for melasma due to lack of superiority compared to hydroquinone [58]. Fractional photothermolysis with a non-ablative 1550-nm laser also improved recalcitrant, blue drug-induced hyperpigmentation of the face secondary to minocycline in a patient who failed treatment with a 1064-nm neodymium YAG (Nd-YAG) laser [59].

**Infectious conditions**

Additionally, FP also appears to have a role as an adjuvant treatment for various infectious conditions. In fact, for treatment of verruca vulgaris, FP and LADD of topical 5% imiquimod cream was shown to have a faster rate of clearance and lower pain scale than conventional treatment with cryotherapy [17]; however, more research is needed in order to determine ideal treatment parameters [60]. Onychomycosis has also been shown to respond better to LADD with topical 28% tioconazole than treatment using topical tioconazole only [19], likely due to the utility of LADD to overcome the nail plate barrier [61]. While there is an emerging role of FP in the treatment of infectious conditions, further research is warranted in this area. We would also like to remind the clinician to be mindful, as FP facilitates transdermal delivery, and this could facilitate the spread of infections under certain circumstances.

**Inflammatory conditions**

Recently, there have been several exploratory studies evaluating the use of fractional lasers for inflammatory skin disease. The fractional ablative 2,940-nm Er:YAG laser has been used in plaque psoriasis to increase penetration of calcipotriol and a novel methotrexate formulation through LADD [21,22].

Active acne and acneiform conditions, including rhinophyma, have also improved with FP. A fractional non-ablative 1320-nm Nd:YAG laser was shown to decrease inflammatory lesion count in acne vulgaris and reduce sebum production in one pilot study [62]. Fractional ablative CO2 lasers, in particular, have shown great promise to improve rhinophyma with decreased lesions and high patient satisfaction, with a better tolerated side-effect profile than traditional surgery or fully ablative procedures [63-65].

Fractional photothermolysis has also been shown to improve granulomatous disorders, including granuloma annulare using a 1440-nm Nd:YAG laser [66], and refractory necrobiosis lipoidica and facial cutaneous sarcoidosis using a fractional ablative CO2 laser [67,68].

Promising results of FP for the treatment of inflammatory skin conditions are notable, as FP may produce paradoxical inflammation during the wound healing response [6] as part of the mechanism to reduce inflammation in the aforementioned conditions. It is possible that through the tissue repair process following fractional skin injury, favourable cytokine modulation may explain the seemingly contradictory effects of fractional lasers on inflammatory skin disease [66]. Further investigation is necessary to elucidate any cellular or molecular mechanisms that may explain how FP has shown promise to improve multiple inflammatory skin conditions.

**Conclusion**

Over the past decade, FP has become more widely used for the treatment of medical dermatology with promising results. Given the broad pathology treated using this concept, it seems that FP treatments have the tendency to ‘normalise’ tissue. This means that similar fractional laser treatments have been shown to remarkably both increase and decrease connective tissue components and pigment towards normal pathology, in addition to promote possible anti-inflammatory and antimicrobial effects. In particular, the unusual capability of FP to induce ‘normalisation’ warrants further investigation, as FP may have the potential to improve additional cutaneous or even internal diseases.

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